



Formulation and Evaluation of Bilayer of Omeprazole Sustained release action

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ABSTRACT

The purpose of present study is to formulate the bilayer tablets containing omeprazole and diclofenac sodium. In this single tablet omeprazole is in immediate release portion and diclofenac sodium is in sustained released portion. This combination of medicine can be used in the person who are at the threat of developing stomach ulcers. Omeprazole act to relieve ulcers and diclofenac manage to relieve pain due to ulcer. Hence, the layered tablets offer a pharmacokinetic advantage over conventional controlled release lozenge forms as the medicine is snappily released from the fast release subcaste leading to rapid-fire rise of medicine tube attention followed by durability of medicine release from the sustained release subcaste. The optimized immediate release subcaste is named from batches OIR9 grounded on medicine release, wetting down time, and decomposition time. The sustained release tablets are optimized using factorial design for dragged medicine release of diclofenac sodium. Floating bioadhesive tablets are prepared using guar goo and xanthan goo as DSR9 expression. The final bilayer tablet expression (BODT1 – BODT9) is prepared using optimized batches from different polymer combinations. The bilayer tablets parade a unique combination of floatation and bioadhesion for prolonged hearthstone in the stomach and quick onset of action. The polymer- to- medicine rate significantly affects floating pause time and medicine release kinetics. Guar goo and xanthan goo also impact swelling indicator, gastric mucosa adhesion, gastric retention, and in- vitro medicine release rate profile. The optimized expression BODT9 is best suited for GRDDS.

Keywords: Bilayer Tablets, Diclofenac sodium, Omeprazole, Drug, Immediate release, Sustained released, Combination, Drug release, Drug release, Tablets

INTRODUCTION

Sustained Release Drug Delivery

The oral controlled release phrasings have several advantages over a conventional system viz. increased patient compliance, reduced dosing frequence, differencing pharmacological exertion and reduced side goods(Allen 2000, Amir 2000). These systems show significant remedial effect. The CR system gives prolonged delivery of active halves at active point or maintains tube medicine situations in remedial range. In addition, by comparing rate of medicine administration with rate of medicine elimination, a steady state medicine situations in tube can be achieved. The utmost of SR systems shows 1st order kinetics where medicine position in tube is further after administration and diminishes exponentially. Easily depicts tube medicines situations upon administrations of IR and CR phrasings.

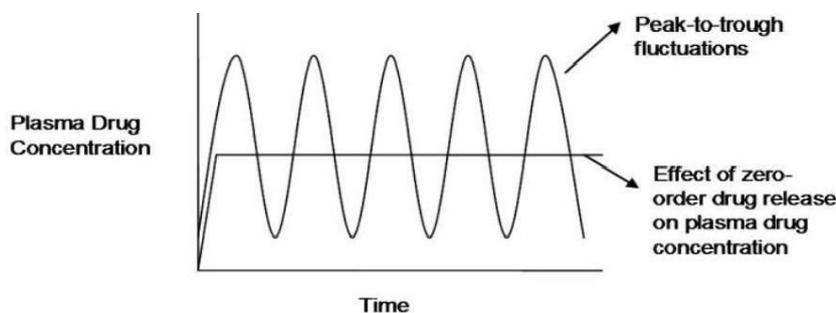


Figure 1.3: Plasma drug level versus time course of conventional and sustained or controlled release formulations

Sustained Medicine release impeccably shows zero order medicine release with extended time of medicine release generally lesser than 12 hours. Several studies are carried out for development of DDS easy to give zero or near zero order release kinetics. From numerous times, the geometric principles have been considered to change medicine release pattern from a non-direct manner to zero or near zero order. The experimenters have tried

HPMCK ₁₅ M	60	60	60	60	60	60	60	60	60	60
Mannitol	10	20	30	40	50	60	70	80	90	100
Micro Crystalline Cellulose	156.5	146.5	136.5	126.5	116.5	106.5	96.5	86.5	76.5	66.5
Talc	1.75	1.75	1.75	1.75	1.75	1.75	1.75	1.75	1.75	1.75
Magnesium stearate	1.75	1.75	1.75	1.75	1.75	1.75	1.75	1.75	1.75	1.75
Total weight (mg)	350	350	350	350	350	350	350	350	350	350

Table: Compositions of Various Verapamil Hydrochloride Osmotic Controlled Release Matrix Tablets with varying Mannitol Concentration

EVALUATION OF PRE COMPRESSION PARAMETERS

- **Organoleptic Identification:**

The drug samples were physically linked i.e. Color, odor and taste etc.

- **Bulk & Tapped Density:**

The medicine greasepaint was exactly counted (M) and poured gently through a glass channel into graduated cylinder and the volume was noted and bulk viscosity was determined. The tapped viscosity was determined using tapped viscosity outfit. A bulk and tapped viscosity of diclofenac sodium is to be 0.309 gm/ ml to 0.311 gm/ ml, and for Omeprazole is to be 0.319 gm/ ml to 0.323 gm/ ml similarly.

- **Partical size**

The average flyspeck size (d_{avg}) of medicine samples were observed by using a phase discrepancy microscope (66172/ Olympus, 100 X, Olympus (India) Pvt. Ltd., New Delhi) fitted with optical micrometer and stage micrometer. The flyspeck size of unmilled diclofenac sodium is to be 33 μm, and for unmilled Omeprazole greasepaint was 51 μm.

- **Flow Properties**

The inflow parcels of medicine maquillages were characterized in terms of carr's indicator, hausner's rate and angle of repose. The Carr's indicator (IC) and Hausner's rate (HR) of medicine maquillages were calculating according to following equation

$$\text{Carr's Index (IC)} = \rho_{\text{Tapped}} - \rho_{\text{Bulk}} / \rho_{\text{Tapped}}$$

$$\text{Hausner's ratio (HR)} = \rho_{\text{Tapped}} / \rho_{\text{Bulk}}$$

$$\text{Angle of repose } (\theta) = \tan^{-1} 2 H / D$$

- **Solubility determination:**

The solubility of both medicines API (Omeprazole) was determined in colorful detergents (Water, 0.1 N HCl, phosphate buffer pH 4.5, phosphate buffer 6.8 and phosphate buffer 7.4). Sodium thiosulphate was added to the medium, when phosphate buffer pH 6.8 and phosphate buffer pH 7.4 were used to avoid oxidation. The fat volume of medicine (Omeprazole) was further to 100 ml of medium and stirred constantly overnight at 37 ± 0.5 °C. The samples were filtered by using Whatman sludge paper (0.45 μm severance size). The solubility assessment of medicine (omeprazole) in 274 nm and 317 nm in different medium was determined spectrophotometrically.

EVALUATION OF POST COMPRESSION PARAMETERS

- **Tablet thickness testing:** The consistence of the tablets (periphery & height) was determined using screw reek.
- **Uniformity of weight of tablet:** Uniformity of weight were determined by tried 20 tablets from each batch and directly counted using an logical balance and average weights were calculated for determination of weight variation.
- **Hardness determination of tablet:** The hardness of tablets is indicates the tensile strength of a tablet. It's expressed in terms of cargo/ pressure needed to crush it when placed on its edge. The tablet hardness was estimated using the Stoke- Monsanto hardness tester. The tablet hardness is expressed in kg.
- **Friability of tablets:** Tablet frangibility test was performed with an average weight of 0.65 g or lower take a sample of whole tablets corresponding to about 6.5 g(20 tablet) at 25 rpm for 4 min using Roches frangibility tester(Model 9509/ ZEC- Z). The chance of frangibility was calculated grounded on the weight lost after the test. A maximum loss of weight(from a single test or from the mean of the three tests) was n't lesser than 1.0.

- **Disintegration test of tablets** The decomposition test was performed using decomposition test outfit(9508/ TEC- 1) Indian Equipment Corp. following the system specified in I.P. etc. using 900 ml of 0.1 N hydrochloric acid.
- **Wetting Study:** doubly folded towel paper was placed in a petri dish having an internal periphery of 5 cm containing 6 ml of water. A immediate release tablets(OIR1- OIR9) was precisely placed on the face of the towel paper in the petri dish. The time needed for water to reach the upper face of the tablet and to fully wet was noted as the wetting time.
- **Swelling Study:** A tablet was counted(W1) and placed in a glass teacup, containing 200 ml of 0.1 N HCl(i.e. pH 1.2), maintained in a water bath at 37 ± 0.5 oC. At regular time intervals, the tablet was taken out and the redundant face liquid was precisely removed by a sludge paper. The study was continued for 8 hrs. The blown tablet was also revisited(W2). The percent lump of sustained release subcaste(DSR1- DSR9) were calculated using the formula. $\% \text{ Swelling} = \{(W2-W1)/W1\} \times 100$
- **Determination of drug content:** Tablets were finely pulverized, and a volume of greasepaint fellow to 50 mg of OMP(OIR1 to OIR9) was directly counted. The counted sample transferred to 100 ml volumetric steins containing roughly 50 ml of 0.1 N HCl result. The steins were shaken for solubilizing the medicine and sonicated for 10 min. The volume was adulterated made up to 100 ml by 0.1 N HCl and mixed completely. The medicine samples were adulterated with same detergent up to 10 µg/ ml. The results were filtered through a 0.45 µm membrane sludge and anatomized for the content at 317 nm for OMP independently using double ray UV spectrophotometer(Shimadzu- 1800).
- **In-vitro drug release study:** IP paddle outfit has been used to study in- vitro medicine release from uncoated tablet. In present study, medicine release was studied using a modified IP dissolution rate test outfit(outfit type II) at 100 rpm in 0.1 N HCl as dissolution fluid(900 ml) maintained at 37 ± 0.5 °C. introverted samples(1 ml) were filtered, anatomized UV spectrophotometrically at 317 nm for OMP independently. The volume was replaced with the same quantum of fresh dissolution fluid each time to maintain the Gomorrah condition.

Result and Discussion

Flow Properties

Table: Flow properties of drug (n = 3)

IR

Drug	Type of powder	Carr's index (%)	Hausner's ratio	Angle of repose θ
Omeprazole	Unmilled	13.08±0.012	1.12±0.021	26.4±0.111
	Milled	10.06±0.016	1.07±0.007	19.2±0.092

Spectrum

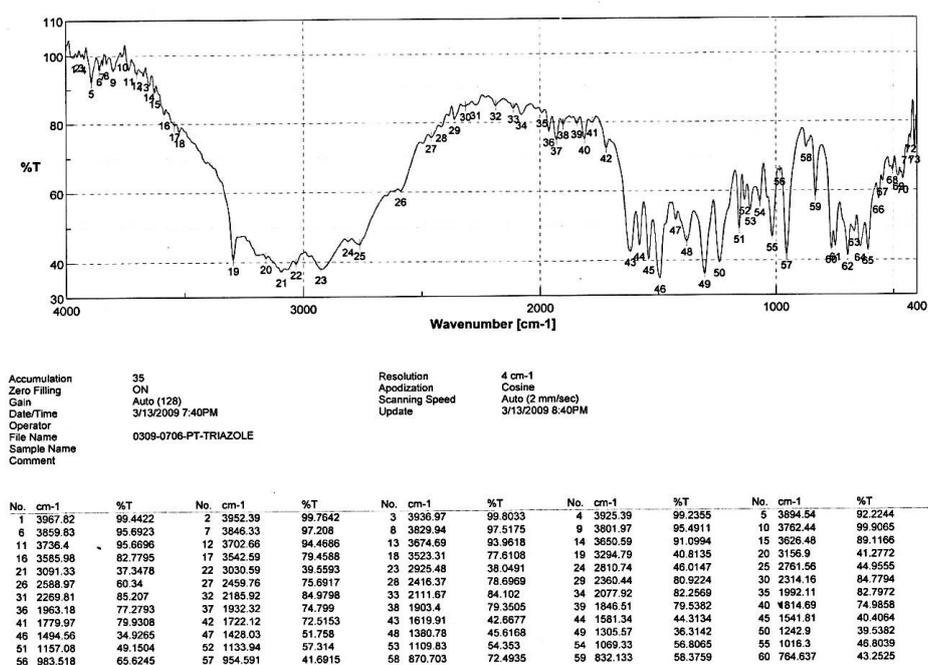


Figure : Infrared spectrum of drug sample (Omeprazole)

Tablet Thickness

Formulation code	Tablet Thickness (cm)	
	Thickness	Diameter
OIR1	0.241±0.001	0.81±0.019
OIR2	0.241±0.002	0.80±0.011
OIR3	0.240±0.003	0.81±0.012
OIR4	0.240±0.001	0.81±0.001
OIR5	0.240±0.001	0.80±0.002
OIR6	0.241±0.001	0.80±0.004
OIR7	0.240±0.003	0.80±0.009
OIR8	0.241±0.003	0.80±0.004
OIR9	0.240±0.003	0.80±0.012

Table : Tablet thickness of immediate release layer

Uniformity of weight

Table: Uniformity of weight of immediate release layer

Formulation code	Average Weight (mg)
OIR1	204.2±0.091
OIR2	198.4±0.011
OIR3	203.2±0.058
OIR4	201.8±0.021
OIR5	208.9±0.018
OIR6	197.1±0.001

Hardness

Table : Hardness determination of immediate release layer

Formulation code	Hardness (kg)
OIR1	3.2±0.39
OIR2	3.8±0.29
OIR3	3.5±0.05

OIR4	3.3±0.13
OIR5	3.3±0.22
OIR6	3.8±0.23

- Friability

Table: Friability determination of immediate release layer

Formulation code	Friability (%)
OIR1	0.381±0.61
OIR2	0.431±0.11
OIR3	0.424±0.32
OIR4	0.435±0.14
OIR5	0.425±0.44
OIR6	0.324±0.24

Disintegration

Table: Disintegration time determination of immediate release layer

Formulation code	Disintegration time (sec.)
OIR1	41±1.7
OIR2	47±2.1
OIR3	59±1.1
OIR4	43±1.7
OIR5	55±2.8
OIR6	51±1.1

Drug Content

Table: Drug content determination of immediate release layer

Formulation code	Drug content (mg)
OIR1	49.03±0.72
OIR2	49.86±1.09
OIR3	49.09±0.01
OIR4	49.11±1.11
OIR5	49.91±0.32
OIR6	49.16±1.19

CONCLUSION

Point specific or targeting medicine to the stomach is set up to be a new approach during last decade. One of the approaches to develop gastro forgetful medicine delivery system which is designed to aim increased gastric hearthstone time of the lozenge form. Among colorful ways to increase gastric hearthstone time; floating bioadhesive is one of them. expression of immediate release subcaste with bioadhesive sustained release subcaste to develop as a bilayer tablet is the new purpose of this disquisition. With the end bilayer tablet is prepared for giving immediate release of omeprazole to attain onset of action snappily i.e. attaining remedial position with many nanoseconds i.e. maintaining remedial position of medicine for asked time period which is over to 12 hrs. Immediate release tablets of omeprazole were originally prepared by using sodium bounce glycolate and sodium lauryl sulphate as a superdisintegrant, microcrystalline cellulose as a diluent. Superdisintegrant promotes the decomposition and eventually dissolution of medicine; accordingly release rate of medicine increases and its immersion led to briskly onset of action. Optimized immediate release subcaste named from batches OIR9 on the base of medicine release, wetting down time & decomposition time. OIR9 was named as optimized immediate subcaste for the expression bilayer tablet. latterly sustained release tablets were optimized on the base of factorial design for dragged medicine release of diclofenac sodium. In this study floating bioadhesive tablets were prepared using guar goo and xanthan goo as DSR9 expression.

REFERENCES:

- Adkin, D. A. (1995). The Effect of Mannitol on the Oral Bioavailability of Cimetidine. *Journal of Pharmaceutical Sciences*, 84(11), 1405–1409.
- Alderman, D. A., & Schulz, G. J. (1989). Method of Making a Granular, Cold Water Dispersible Coating Composition for Tablets. United States Patent, 4,816,298.
- Allen, L. V. (2000). Featured Excipient: Capsule and Tablet Diluents. *International Journal of Pharmaceutical Compounds*, 4(4), 306–310.
- Anschütz, M., Wonnemann, M., Schug, B., Toal, C., Donath, F., Pontius, A., Pauli, K., Brendel, E., & Blume, H. (2010). Differences in Bioavailability Between 60Mg of Nifedipine Osmotic Push-Pull Systems After Fasted and Fed Administration. *International Journal of Clinical Pharmacology and Therapeutics*, 48(2), 158-170.
- Ansel, H. C., Allen, L. V., & Popovich, N. G. (2000). *Pharmaceutical Dosage Forms and Drug Delivery Systems*. Lippincott Williams & Wilkins.
- Banker, G. (1981). Evaluation of Hydroxypropyl Cellulose and Hydroxypropyl Methyl Cellulose as Aqueous Based Film Coatings. *Drug Development and Industrial Pharmacy*, 7, 693–716.
- Bashir, I., Ayesha, S., Zaman, M. D., Qureshi, J., Rai, M. A., Asif, M. D., Sajid, M. D., & Akram, M. D. (2014). Formulation and In-Vitro Bioequivalence Evaluation of Verapamil Hydrochloride Matrix Tablets. *International Current Pharmaceutical Journal*, 3(6), 286-290.
- Bertil, A., Magne, A., Bjorn, B., Ulf, E. J., Maria, E. L., & Annhild, L. (1998). Drug Absorption from Nifedipine Hydrophilic Matrix Extended release (ER) Tablet - Comparison with an Osmotic Pump Tablet and Effect of Food. *Journal of Controlled Release*, 52, 301–310.
- Bhupendra, G., Prajapati, K., Anand Kumar, M., & Visnu, P. (2009). Controlled Release Gastroretentive Dosage Form of Verapamil Hydrochloride. *International Journal of Pharmaceutical Technology and Research*, 1(2), 215-221.
- Bistra, K., & Dimitar, R. (2007). New Co-Polymer Zwitterionic Matrices for Sustained Release of Verapamil Hydrochloride. *Acta Pharm.*, 57, 429–439.
- Bodmeier, R., & Paeratakul, O. (1994). The Effect of Curing on Drug Release and Morphological Properties of Ethylcellulose Pseudolatex-Coated Beads. *Drug Development and Industrial Pharmacy*, 20(9), 1517–1533.
- Bouffard, J. (2005). Influence of Processing Variables and Physicochemical Properties on the Granulation Mechanisms of Mannitol in a Fluid Bed Top Spray Granulator. *Drug Development and Industrial Pharmacy*, 31, 923–933.

13. Chilamkurti, R. N. (1982). Some Studies on Compression Properties of Tablet Matrices Using a Computerized Instrumented Press. *Drug Development and Industrial Pharmacy*, 8, 63-86.
14. Cooper, C. B. (1983). Cellulose Granuloms in the Lungs of a Cocaine Sniffer. *British Medical Journal*, 286, 2021-2022.
15. Cortese, R., & Theeuwes, F. (1982). Osmotic Device With Hydrogel Driving Member. US Patent, 4,327,725.
16. Costa, P., & Lobo, J. M. S. (2001). Modeling and Composition of Dissolution Profile. *European Journal of Pharmaceutical Sciences*, 13, 123-133.
17. Dahl, T. C. (1990). Influence of Physicochemical Properties of Hydroxypropylmethylcellulose on Nifedipine Release from Matrix Tablets. *International Journal of Pharmaceutics*, 64(1-2), 207-216.
18. Davis, A. M. (1999). Biopharmaceutics and Clinical Pharmacokinetics of Flavopiridol. *Clinical Pharmacokinetics*, 36(3), 193-212.
19. Desai, M. J., Parikh, J. R., Parikh, R. H., & Patel, V. B. (2009). Design and Development of Controlled Release Tablets of Nifedipine. *Journal of Pharmaceutical Sciences and Research*, 1(3), 116-120.
20. Ding, H., & Kopeckova, P. (2004). Self-Association Properties of Water-Soluble Polymers. *Macromolecules*, 37(23), 8675-8680.
21. Dixit, R. P., Puthli, S. P., & Pancholi, S. S. (2005). Gastroretentive Drug Delivery Systems: A Review. *Indian Journal of Pharmaceutical Sciences*, 67(3), 265-274.
22. Eckenhoff J. B., & Thalhammer, J. G (1985). Pharmacokinetics and Pharmacodynamics of Atracurium in Humans. *Anesthesiology*, 62(4), 388-394.
23. Endoh, T., Tajima, M., & Suzuki, T. (1981). Rate of Release of Theophylline from Theophylline Sustained Release Formulations. *Journal of Pharmacobio-Dynamics*, 4(7), 523-528.
24. Faigle, J. W. (1996). A Process for Preparing Microporous Multiparticulate Tablets. United States Patent, 5,547,688.
25. Flickinger, J. G., & Heacock, A. M. (2007). Pharmaceutical Compositions for the Coordinated Delivery of NSAIDs. United States Patent, 7,220,422.
26. Gabor, U., & Janos, T. (1991). Gastrointestinal Sustained Release Granules. United States Patent, 4,985,253.
27. Gautam, C. S., & Jain, S. K. (1997). Oral Controlled Release Formulations: Some Success Stories and Opportunities for the Future. *Critical Reviews in Therapeutic Drug Carrier Systems*, 14(2), 113-155.
28. Gedye, R. N., Smith, F., Westaway, K., Ali, H., & Baldisera, L. (1986). The Use of Microwave Ovens for Rapid Organic Synthesis. *Tetrahedron Letters*, 27(3), 279-282.
29. Giunchedi, P., Gavini, E., Moretti, M. D., Pirisino, G., & Cossu, M. (2000). Rivastigmine Biodegradable Microspheres: Effect of Some Manufacturing Parameters.
30. Hanna, C. (2003). Osmotic Drug Delivery: A Review of the Patents. *Recent Patents on Drug Delivery & Formulation*, 5(3), 195-200.
31. Hussain, A., Samad, A., Ramzan, M., & Ahsan, H. (2010). Nanoemulsion Gel-Based Topical Delivery of an Antifungal Drug: In Vitro Activity and In Vivo Evaluation. *Drug Development and Industrial Pharmacy*, 36(7), 764-774.